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Role of intravoxel incoherent motion difusion-weighted MRI in diferentiation of renal cell carcinoma subtypes

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Abstract

Background Renal cell carcinoma is the most fatal form of renal tumors, representing about ninety percent of all renal cancers. There are diferent variations in prognosis among various histological types of RCC. In recent years, there has been a greater emphasis on diferentiating between RCC subtypes. Evaluation of diferent subtypes of renal cell carcinoma using intravoxel incoherent motion (IVIM) difusion-weighted MRI is the aim of this study.

Results Clear cell renal cell carcinoma (CCRCCs) showed highest f and D values, followed by chromophobe renal cell carcinoma (ChRCCs), while papillary renal cell carcinoma (PRCCs) had the lowest values. CCRCCs had signifcantly diferent D and f values compared to non-clear types (PRCC and ChRCC) (*P*<0.05). The D* values of CCRCC were the highest, PCRCC had intermediate values, while ChRCCs had the lowest values (*P*<0.05). The D* values of ChRCCs demonstrated signifcant diference when compared to both CCRCCs and PRCCs (*P*<0.05). The cutof points of D, D* and f parameters for distinguishing CCRCCs from non-clear cell types (ChRCCs and PRCC) were 0.835, 0.0355 and 0.335, respectively, yielding specifcities of 97.2%, 83.3% and 76.5% and sensitivities of 100%, 57.5% and 72.7%, respectively.

Conclusion Intravoxel incoherent motion (IVIM) can be utilized to distinguish renal cell carcinoma subtypes.

Keywords Kidney, Renal cell carcinoma, IVIM MRI

Background

Renal cell carcinoma (RCC) is a multiple variety of tumors that originates from the epithelium of the renal tubules. It is considered as a group of illness with discrete histological types, molecular and genetic variations with distinct clinical prognosis [[1\]](#page-9-0).

Clear cell, papillary and chromophobe RCCs are the most predominant subtypes of RCC, constituting approximately 75%, 15% and 5% of RCCs cases, respectively.

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Diferentiation of renal masses is useful in distinguishing those that require active surveillance or ablation from those requiring surgery without the need for biopsy [\[4](#page-9-3)]. Histological classifcation of RCC is performed preoperative by invasive methods through percutaneous biopsy. Recently, a large number of studies have documented the value of imaging in the non-invasive evaluation of diferent RCC subtypes [\[5](#page-9-4)].

Non-invasive techniques, such as MRI, have been thoroughly detailed in the assessment of common frequent subtypes of RCC $[6]$ $[6]$. Both diffusion-weighted imaging (DWI) and apparent diffusion coefficient (ADC) measurements were extensively utilized in the characterization

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as well as identifcation of renal masses [\[7,](#page-9-6) [8](#page-9-7)]. However, the ADC is determined with a monoexponential model and does not adequately refect the difusion factor of tissues as it involves the impacts of perfusion (the capillaries microcirculation of blood) and difusion (water molecules movement inside tissue) [[9\]](#page-9-8).

Intravoxel incoherent motion (IVIM) DWI, initially documented by Le Bihan et al., uses the biexponential model with several b values to calculate both tissues diffusion and perfusion, independently [[9\]](#page-9-8). Main IVIM parameters include true diffusion coefficient (D), pseudodiffusion (D^*) and perfusion fraction (f) that represent the tissue true molecular difusion, perfusion of blood capillary microcirculation and the microcapillary perfusion fraction, respectively [[9,](#page-9-8) [10\]](#page-9-9).

IVIM MRI is sensitive to both molecular difusion in tissues and to microcirculation (perfusion) based on the assumption that the flow of blood through capillaries mimics a difusion process, due to the pseudo-random organization of capillaries in tissue [[11\]](#page-9-10). Microcirculation contributes greatly to the difusion-weighted MRI signal together with genuine water molecule difusion in tissues [[12,](#page-9-11) [13](#page-9-12)].

A key advantage of IVIM MRI is ability to give quantitative data about microcirculation without using contrast agents, a signifcant beneft in terms of price, acquisition times and suitability for patients who are contraindicated to receive gadolinium-based contrast agents [[14,](#page-9-13) [15\]](#page-9-14).

Methods

- This prospective study was done from May 2023 to December 2023. All cases were referred to our radiology department at urology and nephrology center from the clinic within the same center. Our study received permission by the institutional board of ethics, and each patient gave his informed consent after being fully informed about the benefts and hazards of the procedure. There were no other obvious hazards to the patients in this study.
- *Inclusion criteria* Patients over the age of eighteen years who had solid renal mass parenchymal in origin that have been identifed by CT or US.
- *Exclusion criteria* Patients who are contraindicated for MRI study (like patient with metallic prostheses or pacemakers), cases who refused consent and cases with no histology results

MRI technique

MRI examination was performed for each patient using a 3 Tesla MRI scanner (Phillips, Ingenia 3 T, Best, The Netherlands). Phased-array body coil using M-Dixon program was utilized in our procedure, and imaging was done in the supine position including these sequences: (T2WI, fat-suppressed T1W sequences, DWI, IVIM). As regards the IVIM, in the axial or coronal planes, we applied single-shot echo-planar imaging sequence using a respiratory belt with eight b values (0, 200, 400, 600, 800, 1000, 1200 and 1400 s/mm2). Other parameters were: 24 slices covering both kidneys, $(TE) = 33.2 \times 86.6$ ms, $(TR) = 1000$ ms, matrix = 96 × 128, FOV = 36 × 36 cm. The mean acquisition time of IVIM sequence was 16.6+3.2 min.

Image analysis

The DICOM pictures were sent to the vendor-supplied workstation (Intellispace portal Workspace 6.0.1 Philips Medical Systems Netherlands B.V). The procedure was done without knowledge of the pathology results. Using IVIM protocol, we got measurements for D , D^* and f. ROIs of the lesion $(100-225 \text{ mm}^2)$ were manually drawn trying to avoid aliasing artifacts appeared in an image, calcifcation inside the mass and cystic degeneration. We obtained three measurements for each parameter, and the average measurement was taken.

Statistical analysis and data interpretation

Version 25 of the SPSS program (SPSS Inc., PASW statistics for windows version 25. Chicago: SPSS Inc.) was used to analyze the data. Numbers and percentages were used to describe the qualitative data. After determining the normalcy of the quantitative data using the Kolmogrov– Smirnov or Shapiro–Wilk tests, the data were presented using the mean±standard deviation for normally distributed data. The results were evaluated for significance at the (≤ 0.05) level.

When comparing more than two independent groups, the one-way ANOVA test was utilized and the post hoc Tukey test was applied to identify pair-wise comparisons. The best cutoff point was determined by calculating the validity (sensitivity & specifcity) of continuous variables using the receiver operating characteristics curve (ROC curve). Using cross-tabulation, predictive values and accuracy are evaluated.

Pathological analysis

Final diagnosis by histopathology was obtained after excision of renal masses surgically by either partial or radical nephrectomy.

Results

Seventy-six patients with renal cell carcinomas confrmed by histology were included in our prospective study (35 females and 41 males). Their age range was $(29-77)$ years with average age that was 53.13 years. We observed no

significant differences for either age $(p=0.81)$ or sex $(p=0.34)$. The distribution of their pathology was 40 clear cell RCCs (52.6%), 22 papillary RCCs (28.9%) and 14 chromophobe RCCs (18.5%) (Fig. [1\)](#page-2-0).

 $(0.751 \pm 0.054 \times 10^{-3} \text{mm}^2/\text{s})$ and lowest for PRCCs $(0.575 \pm 0.043 \times 10^{-3} \text{mm}^2/\text{s})$ $(0.575 \pm 0.043 \times 10^{-3} \text{mm}^2/\text{s})$ $(0.575 \pm 0.043 \times 10^{-3} \text{mm}^2/\text{s})$ (Figs. 2, [3](#page-3-0)). The D parameter showed also high statistically signifcant diference in diferentiating clear cell type from non-clear cell types including both chromophobe & papillary types, $p < 0.001$ for both (Table [1\)](#page-3-1). The area under curve for Diffusion coefficient (D) was excellent ($AUC=1.0$), and the cutoff point of D value was≥0.835 for distinguishing CCRCCs from non-clear cell types (ChRCCs and PRCCs) with sensitivity of 100% and specificity of 97.[2](#page-3-2)% (Table 2), (Figs. [6,](#page-5-0) [7](#page-6-0), [8\)](#page-7-0).

Regarding the D* parameter, CCRCCs also had the highest D^* values $(0.035 \pm 0.006 \text{ mm}^2/\text{s})$ followed by PRCCs $(0.033 \pm 0.002 \text{ mm}^2/\text{s})$ and lowest for ChRCCs $(0.022 \pm 0.004 \text{ mm}^2/\text{s})$ (Figs. 2, 4). Statistically significant diference was detected among CCRCCs & ChRCCs types and between PRCCs & ChRCCs (*P*<0.001 for both), but no statistically signifcant diference was detected between CCRCCs & PRCCs (*p*=0.084) (Table [1\)](#page-3-1). AUC for pseudo-diffusion (D^*) is good $(AUC=0.745)$, with the best detected cutoff point for differentiating CCRCCs from non-clear cell types (ChRCCs and PRCCs) that is≤0.0355 yielding sensitivity of 57.5% and specifcity Fig. 1 Histopathology of the studied cases 83.3% (Table [2\)](#page-3-2), (Figs. [6](#page-5-0), [7,](#page-6-0) [8](#page-7-0)).

Fig. 2 The mean values for D, D^{*} and f among the three subtypes, CCRCC, PRCC and ChRCCs. D diffusion coefficient, D^{*}pseudo-diffusion, f perfusion fraction, CCRCC clear cell renal cell carcinoma, PRCC papillary renal cell carcinoma, ChRCCs chromophobe renal cell carcinoma

Fig. 3 Boxplot shows the diference between clear cell, papillary and chromophobe RCCs measurements according to the D parameter within the studied groups. The D values were highest for CCRCC (1.44±0.19×10⁻³mm²/s) followed by ChRCCs (0.751+0.054×10⁻³mm²/s) and lowest for PRCC (0.575 + 0.043 × 10^{−3}mm²/s). D diffusion coefficient, CCRCC clear cell renal cell carcinoma, ChRCCs chromophobe renal cell carcinoma, PRCC papillary renal cell carcinoma

Parameters described as mean±SD.*statistically signifcant, P1: diference between clear & papillary carcinoma group, P2: diference between clear and chromophobe, P3: diference between papillary & chromophobe

Table 2 Validity of D, D* and f in differentiating clear cell type (CCRCC) from non-clear cell types (ChRCCs & PRCC)

	AUC (95%CI)	P value	Cutoff point	Sensitivity %	Specificity %
	$1.0(1.0-1.0)$	$< 0.001*$	≥ 0.835	100.0	97.2
D^*	$0.745(0.635 - 0.856)$	$< 0.001*$	≥ 0.0355	57.5	83.3
	$0.823(0.728 - 0.917)$	$< 0.001*$	≥ 0.335	72.,	76.5

The f values were highest for CCRCCs $(0.449 \pm 0.16\%)$ followed by ChRCCs $(0.347 \pm 0.07%)$ and lowest for PRCCs (0.286±0.045%) (Figs. [2](#page-2-1), [5\)](#page-4-1). Statistically signifcant diference was detected between CCRCCs & PRCCs (P1<0.001) and between CCRCCs & ChRCCs (P2<0.008), but no statistically signifcant diference was detected between ChRCCs & PRCCs (P3=0.139) (Table [1\)](#page-3-1). Area under curve for perfusion fraction (f)

Fig. 4 Boxplot shows the difference between clear cell, papillary and chromophobe RCCs measurements according to the D* parameter within the studied groups. The D* values were highest for CCRCCs (0.035 \pm 0.006 mm²/s) followed by PRCCs (0.033 \pm 0.002 mm²/s) and lowest for ChRCCs (0.022±0.004 mm2 /s). D* difusion coefcient, CCRCC clear cell renal cell carcinoma, ChRCC chromophobe renal cell carcinoma, PRCC papillary renal cell carcinoma

Fig. 5 Boxplot shows the diference between clear cell, papillary and chromophobe RCCs measurements according to the f parameter within the studied groups. The f values were highest for CCRCCs (0.449±0.16%) followed by ChRCCs (0.347±0.07%) and lowest for PRCCs (0.286±0.045%). f perfusion fraction, CCRCC clear cell renal cell carcinoma, ChRCC chromophobe renal cell carcinoma, PRCC papillary renal cell carcinoma

was excellent ($AUC=0.823$), with the best detected cutof point for diferentiating CCRCCs from non-clear cell types (ChRCCs and PRCCs) that is≤0.355 yielding sen-sitivity of 7[2](#page-3-2).7%, specificity 76.5% (Table 2), (Figs. [6](#page-5-0), [7,](#page-6-0) [8](#page-7-0)).

Discussion

Renal cell carcinoma is the most fatal form of renal tumors, representing about ninety percent of all renal cancers, and its incidence increases annually by about

Fig. 6 A 63-year-old male patient presented with left lower polar soft tissue mass confrmed as clear cell RCC by histopathology. **A** Coronal T2WI showing heterogenous SI of the renal mass. **B–D** Showing D, D* and f maps with measured values as 1.23 × 10–3 mm²/s, 0.028 mm²/s and 0.43%, respectively. **E** ROC curve of D, D* & F in diferentiating clear cell RCC from non-clear cell types (ChRCC & PRCC)

 $2-3\%$ [\[16](#page-9-15)]. The most predominant subtype of RCC is clear cell type, representing about 75%. It is also the worst form of RCCs regarding its prognosis with fveyear survival rate ranging from 44 to 69% [[3,](#page-9-2) [17\]](#page-9-16).

Multiparametric MRI has recently become the most reliable method for diferentiation of renal tumors, yet other advanced MRI techniques are still required to evaluate renal tumor subtypes. ADC is a quantitative method determined from MR-DWI images that is afected by numerous physiological and pathological states of the renal system [\[18](#page-9-17)].

IVIM can be done without the need of contrast agents' injection to ofer a distinctive image of the tissue perfusion. The proportion of tumor tissue cellularity and

Fig. 7 A 52-year-old male patient presented with right lower polar soft tissue mass confrmed as papillary RCC by histopathology. **A** Coronal T2WI showing heterogenous SI of the renal mass. **B–D** Showing D, D* and f maps with measured values as 0.53 × 10–3 mm²/s, 0.031 mm²/s and 0.22%, respectively. **E** ROC curve of D, D* & f in diferentiating papillary RCC from other types (CCRCC & ChRCC)

vascularity varies between renal tumor types; therefore, the IVIM parameters including D, D* and f can represent diferent issues that operate within ADC and can ofer accurate and sensitive assessment of renal masses [[13\]](#page-9-12).

The random microscopic movement of water molecules in extra- or intracellular spaces as well as in the blood microcirculation that arises in each voxel on MR images

is refected by IVIM [\[9](#page-9-8)]. IVIM theory suggested that a number of tissue characteristics, such as the existence of restricting barriers inside the tissue, the fuid consistency in which the spinning molecules are spreading, the speed and fractional volume of perfusing spins all have an impact on perfusion and difusion [\[11\]](#page-9-10).

Fig. 8 A 48-year-old male patient presented with right upper polar soft tissue mass confrmed as chromophobe RCC by histopathology. **A** Coronal T2WI showing intermediate SI of the renal mass. **B–D** Showing D, D* and f maps with measured values as 0.73 x 10–3 mm²/s, 0.023 mm²/s and 0.29%, respectively. **E** ROC curve of D, D* & f in diferentiating chromophobe cell RCC from other types (CCRCC & PRCC)

Assessment of renal tumors is beneficial in determining masses that require surgical excision with no further assessment by biopsy from masses that need active surveillance or ablation $[19]$ $[19]$. Therefore, we conducted this prospective study, with the primary aim that is to assess role of IVIM in renal cell carcinomas characterization and diferentiation in correlation with histopathology subtypes.

In our study, CCRCCs showed the highest D values followed by ChRCCs and lowest for PRCCs. The D parameter showed also high signifcant statistical diference between clear cell type and both chromophobe & papillary types, *P*<0.001 for both with the best detected cutoff value for discrimination of clear cell types versus non-clear cell types is ≥0.835 with $(AUC=1.0)$ yielding sensitivity of 100.0% and specifcity 97.2%. Tissue cellularity and perfusion have an impact on the D values. It was reported that lower D values have been correlated to greater cellularity in several studies [\[20](#page-9-19)]. Also, the lower D values could be caused by the viscosity of the tumor or mechanical restriction of water difusion by barriers such cell membranes. The cells of clear cell RCC are rich in phospholipids, cholesterol and neutral lipids. Moreover, tumor cells of CCRCCs are separated by interstitial spaces and have hemorrhagic and cystic areas, which allowed water to spread freely [[21\]](#page-9-20).

As regard the f parameter, it nearly showed the same results as the D parameter, its values were high within CCRCCs, moderate within ChRCCs and low within PRCC, but we found significant statistical difference among CCRCCs & PRCCs (*P*<0.001), as well as CCRCCs & ChRCCs (*P*<0.008). But signifcant statistical difference noticed among PRCCs & ChRCCs (*P*=0.139) with best detected cutoff value for discrimination of clear cell types versus non-clear cell types that is ≤ 0.355 $(AUC=0.823)$, resulting in sensitivity about 72.7% and specificity about 76.5%.

Comparable to our fndings, Zhu, Qingqiang et al. 2019 mentioned that the f and D values were high within CCRCCs, moderate within ChRCCs and low within PRCC. The D values of CCRCCs showed significant statistical diference among ChRCCs and PRCCs (*P*<0.05) with f and D measurements of 0.41 and 1.10, respectively, as the cutoff value for distinguishing CCRCCs versus both PRCCs and ChRCCs [[22\]](#page-9-21).

Our results detected that the CCRCCs had also the greatest D* values, but moderate values were detected among PRCCs and least values detected among ChRCCs. Signifcant statistical diference was detected among CCRCCs & ChRCCs types as well as among PRCCs & ChRCCs $(P<0.001$ for both). However, no significant statistical diference was detected among CCRCCs & PRCCs $(p=0.084)$ with best detected cutoff value to diferentiate CCRCCs from ChRCCs and PRCCs that is ≤0.0355 (AUC = 0.745) yielding sensitivity of 57.5% and specificity 83.3%. D^* values may be influenced by capillary density and vascular perfusion. The tissue capillary density is probably the reason for rising D^* values as clear cell RCCs are hypervascular renal tumors [\[23](#page-9-22)].

Our results are on the same level of agreement with **Ding, Yuqin, et al.,2016 study**; they mentioned that the three subtypes of RCCs had signifcant statistical diference for D^* and D (all $p < 0.050$) and also mentioned that CCRCCs exhibited the greatest D values. Regarding the f values their results suggested that CCRCCs had greater

f values in comparison with non-CCRCCs $(p<0.05)$ [[24\]](#page-9-23). Contrary to our fndings **Chandarana, Hersh, et al.,2012**, they reported that f parameter had higher accuracy versus D parameter $(AUC=0.74)$ to diagnose clear cell type, but the utilization and measurements of both f and D parameters together had the greatest accuracy (AUC = 0.78) [25].

Our research is subject to some limitations: First, the number of cases was not large and only limited number of cases enrolled within every subgroup, this might infuence the reproducibility and validity of the fndings, so larger sample size may be necessary to ensure our results. Second, the cases enrolled in the study were not refective of majority of people because the research had enrolled only patients who were referred to a specialized center, which may have resulted in a biased sample. Third, there was a possibility of false(-ve) results as we might miss small foci of the tumor. Finally, our study may have lacked continuous surveillance to assess patients' clinical outcomes. For example, the study may have assessed the diagnostic accuracy of IVIM, but not its ability to predict the prognosis.

In summary, this study clarifed that IVIM parameters difer signifcantly among renal cell carcinoma subtypes. This approach may be used as a non-invasive technique for diferentiating between renal cell cancer subtypes. Even so, we cannot replace percutaneous biopsy by these radiological fndings as there is major overlapping among diferent renal tumors.

Conclusions

In conclusion, the current study showed that IVIM quantitative parameters show the potential to favor the RCC diagnosis and characterization. It may be a hopeful method for assessment of the pathological alterations of RCC tissue, such as predict CCRCC versus non-CCRCC subtypes.

The current study has found that D value varies majorly among diferent subtypes of CCRCC which may refect diferences in tissue microstructure and cellular density between them and can be elucidated with RCC hypercellularity. IVIM, when used with routine MRI of kidney may be valuable in improving the specifcity and the sensitivity of detection of RCC particularly combined D, D* & f showed good to excellent non-invasive diagnostic accuracy in diferentiating subtypes of RCC potentially reducing the need for invasive procedures such as biopsies.

Abbreviations

- MRI Magnetic resonance image
- IVIM Intravoxel incoherent motion

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Author contributions

AM contributed to the data collection. AM and AE performed data analysis and writing. AE, NF and EH performed supervision. They all approved the fnal revision of the manuscript.

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Availability of data and materials

The datasets used and/or analyzed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

This study was approved by the Research Ethics Committee of the Faculty of Medicine at Mansoura University in Egypt on 06/03/2023; reference number of approval: (MS.23.02.2297).

Consent for publication

All patients included in this research gave written informed consent to publish the data contained within this study.

Competing interests

The authors declare that they have no competing interests.

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