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MRI evaluation of hepatic and cardiac iron burden in pediatric thalassemia major patients: spectrum of findings by T2*



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Abstract

Background: Iron deposition distorts the local magnetic field exerting T2* signal decay. Biopsy, serum ferritin, echocardiography are not reliable to adjust iron chelation therapy. Quantified MRI signal decay can replace biopsy to diagnose iron burden, guide treatment, and follow up. The objective of this study is to evaluate the role of T2* in quantification of the liver and heart iron burden in thalassemia major patients. This cross-sectional study included 44 thalassemia patients who were referred to MRI unit, underwent T2* MRI.

Results: Twenty-one male (47.7%) and 23 female (52.3%) were included (age range 6–15 years, mean age 10.9 \pm 2.9 years). Patients with excess hepatic iron show the following: 11/40 (27.5%) mild, (13/40) 32.5% moderate, and (14/40) 35% severe liver iron overload. High statistical significance regarding association between LIC and liver T2* (p = 0.000) encountered. Cardiac T2* values showed no relationship with age (p = 0.6).

Conclusion: T2* is a good method to quantify, monitor hepatic and myocardial iron burden, guiding chelation therapy and prevent iron-induced cardiac complications.

Keywords: Thalassemia major (TM), Liver iron concentration, T2*

Background

Thalassemia major (TM) patients require regular blood transfusions which may lead to iron overload. Excess iron is accumulated in the liver, heart and endocrine organs. Intracellular free iron can cause tissue damage, leads to arrhythmias, heart failure accounting for 71% of deaths in TM patients [1–4].

Significant cardiac iron load can be encountered, although the hepatic iron concentration is kept low, an issue urges the need to quantify this burden, especially in a non-invasive manner in the pediatric age group [5].

Instead of measuring the serum ferritin level (a metalloprotein found in the cells) to take a tissue biopsy to diagnose iron overload, $T2^*$ can be used as a non-invasive method [6]. $T2^*$ is useful in tailoring the iron chelation strategies [7, 8].

Assessing the T2 and T2* relaxation parameters is the gold standard in cases of iron overload. Iron is not directly imaged, instead, water protons are imaged so long they diffuse near iron deposits in the tissue of interest. Those iron particles with their characteristic ferromagnetic effects act as small magnets, destroying the homogeneity of the magnetic field in iron-laden tissues, so moving water protons significantly exhibit different magnetic momentum and desynchronized from each other. A consequence yields a black image by a rate proportional to the iron load [3, 4]. The objective of this work is to evaluate the role of T2* in detection and quantification of cardiac and hepatic iron concentration in pediatric TM transfusion-dependent patients.

Methods

Study design and population

This prospective cross-section study included 44 thalassemia pediatric patients from 6 to 15 years old. They were referred from the pediatric department to radiodiagnosis department from February 2015 to January 2019 after getting a local institutional review board (IRB)

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approval and informed consents from all patients' parents before the study.

Inclusion criteria were pediatric TM patients receiving a regular blood transfusion and iron chelation agent (Ferriprox). Cases of siderotic cardiomyopathy or have potential contraindications to MRI examination including claustrophobia, metallic objects, and pacemakers were excluded. Patients were subjected to MRI examination after thorough history taking (regarding patient's chelation regimen, serum ferritin level and echocardiographic findings).

Patient preparation

MRI examinations were done using a 1.5 Tesla superconducting magnet (Achieva, Philips Medical System, Best, Netherlands). Fasting and sedation were not needed prior to the exam. Respiratory triggering was applied to ensure minimal movement and lessen respiratory motion artifact. In cases of free-breathing, increased signal averaging number to 3 was used (instead of 1 at breath-holding technique).

Scan protocol and parameters

Cardiac gating MRI exam was performed in a supine position with head first using torso phased-array body coil. The field of view (FOV) extends from the carina caudally to the lower renal pole.

The MR protocol is as follows: time of exam is 25–40 min including time spent on instructing the patients.

- 3-plane localizer. (Ensure the heart at the center of the field).
- Cardiac T2* (Table 1): scanned at 8 different echo times (TE 1.5, 4, 6.4, 8.8, 11.2, 13.6, 16, and 18.5 ms).
- The following two sequences were used: single breath-hold multi-echo gradient echo sequence (white blood) and double inversion recovery 'black blood' sequence where TI should be set to extend into diastole and the blood signal should be

Table 1 Parameters for cardiac T2* imaging

Parameter	Value
Slice thickness	10 mm
FOV	40 cm
Flip angle	20
Matrix	128 × 256
TE	1.5–18.5 with 2.4 ms increments
TR	99–125 ms
Bandwidth	810 Hz/pixel
Flow compensation	On
Fat saturation	Off

adequately nulled thus reducing the blood flow artifact and motion artifact.

Mid ventricular imaging plane using 2 chamber, 4 chamber, and short-axis images (usually mid papillary muscle level) was selected not encroaching on the outflow tract. To minimize the breath-hold time we used in plane rotation and reduced the field of view in phase encoding direction.

Liver T2* (Table 2): the acquisition consists of 5 slices collected through the center of the liver in a single breath-hold at 16 different echo times (TE 1, 1.9, 2.7, 3.6, 4.4, 5.3, 6.1, 7, 7.8, 8.7, 9.5, 10.4, 11.3, 12.2, and 13.1 ms) with a gradient-echo sequence (Turbo field echo: TFE) to ensure accurate measurement of liver T2* in cases with light liver iron burdens.

We used large voxels to improve the signal to noise ratio and so decreased echo time. Voxels are 4-5 mm in-plane resolution. According to body habitus FOV was adjusted (FOV < 32 cm may prolong the echo time).

Thin slice axial T2 (Table 3)*: provides a finer sampling of the entire abdomen extending from diaphragm dome to the lower renal poles. Slice positioning should have some slop to account for variable breath-hold position. Voxel size should have 2–3 mm in-plane resolution. It takes five stacks to span the target region. TR was reduced to increase coverage to five slices per breath-hold.

Before the patient's departure. The MRI technician must review the image data after scans are completed to avoid recalling the patient later for a repeat MRI.

Image analysis

Patient data were removed automatically from the DICOM meta-data by Image Inbox prior to image transfer. All MR images were sent to an advanced

Table 2 Parameters for liver T2* imaging

Table 2 Farameters for liver 12 limaging			
Parameter	Value		
Slice thickness	10 mm		
#Slices/#slices per BH	5/5		
FOV ($F \times Ph$)	40 × 24		
Flip angle	20		
Frequency matrix	96–128		
Phase matrix	64–96		
TE	1–13.1 ms with 0.9 ms increments		
TR	100 ms		
Bandwidth	Min water-fat shift 810 Hz/pixel		
Pulse sequence	TFE		

Table 3 Parameters for axial T2* imaging

Value
5 mm
15–25/5
32-36 × 24-27
20
96–128
64–96
1–13.1 ms with 0.9 ms increments
100 ms
Min water-fat shift 810 Hz/pixel
TFE

workstation (Philips MR extended workspace, software version 2009). The data sets were typed to liver and heart spreadsheets. The T2*, R2*, LIC, and MIC were automatically calculated from the datasets [9–13] included in the analyses. Heart and liver plot charts were generated and final results were represented in colored manner based on the severity of iron burden; while green refers to normal values, mild affection is presented in yellow, moderate in orange, and severe in red color. All images were checked and analyzed by two radiologists (who were blinded regarding the laboratory, clinical situation of the patient and echocardiography results) as follows:

- Cardiac MR-T2* values were quantified with the region of interest in the ventricular septum to avoid susceptibility artifact. The region of interest was copied automatically to identical positions on images from different TEs (Fig. 1). Patients with iron-loaded heart showed rapid signal loss with increasing TE with both black and white blood sequences and T2* measures were less than 20 ms. They were categorized as mild (15–20 ms), moderate (10–15 ms), and severe (T2*; < 10 ms) [14].
- Myocardial iron concentration (MIC) was also calculated from R2* using the equation (0.0254 × R2*) + 0.202 (R2*, the reciprocal of T2*, 1000/T2*), according to carpenter JP et al. formula [15] where values from 1.16 to 1.65 indicate light, 1.65 to 2.71 indicate moderate, and more than 2.71 mg/g indicate severe cardiac siderosis.
- Liver-T2* values below 11.4 ms indicate iron overload: mild (3.8–11.4), moderate (1.8–3.8), and severe (> 1.8 ms).
- Liver iron concentration (LIC) using Garbowski MW et al. formula [16] was calculated where 2–7 mg/g indicates light, 7 to 15 indicate moderate, and <15 mg/g severe iron burden.

Echocardiography

It was performed within 1 week from MRI by a pediatric cardiologist who was blinded to the clinical data and imaging results to evaluate the cardiac function owing to

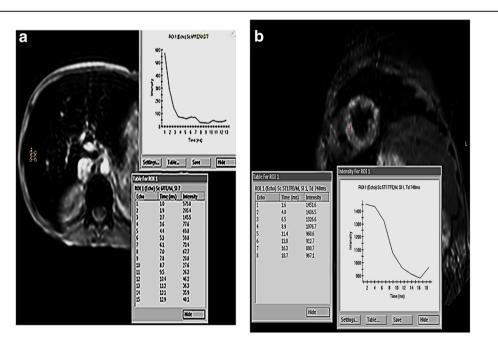


Fig. 1 Time-signal intensity curves delivered from ROI positioned in the right liver lobe (a) and interventricular septum (b) at 15 different TE (1.1-12.9ms) for the liver and 8 different TE (1.6-18.7ms) for the heart

Table 4 Correlation between serum ferritin, hepatic, and cardiac investigations of the studied group

Variable	Serum ferriti	n	
	r ^{\$}	р	SIG
Cardiac T2*	- 0.1	0.4	NS
MIC	0.2	0.1	NS
Hepatic T2*	- 0.4	0.02*	S
LIC	0.5	0.01*	S

NS not significant; S significant

Both Hepatic T2* & LIC have p values <0.05 so both are statistically significant

the unavailability of MRI software for cardiac function assessment in our department. The parameters tested were diastolic and systolic functions. An ejection fraction >55% and >27% fraction shortening was considered as normal systolic function; while E/A ratio less than 1 was considered as normal diastolic function.

Serum ferritin level

It was performed as a primary screening test to evaluate the iron overload.

Statistical analysis

The data analysis was performed using SPSS 20 (Chicago SPSS, SPSS Inc., Chicago, IL). Comparison of cardiac T2*, MIC, and hepatic T2* and LIC values was performed with Kruskal-Wallis test. We used the Spearman test to correlate between serum ferritin level and T2*, MIC, and LIC. A p value of < 0.05 reflects a statistical significance.

Results

This study included 44 pediatric TM patients (21 male; 47.7 % and 23 female; 52.3 %). Only 40 (18 males; 45% and 22 females; 55%) patients performed cardiac MRI and completed the study, their age ranges from 6 to 15 years with a mean 10.9 ± 2.9 years. Remaining 4 patients were excluded due to poor quality cardiac images from motion artifact. All patients received Ferriprox as iron chelator agent.

All subjects had a high serum ferritin (ranging from 1000 to 7000 ng/ml) with a mean 3141.2 ± 1967.5 . Only 35/40 patients performed echocardiography and all patients had normal or accepted echocardiographic results regarding the diastolic and systolic functions.

Table 5 Association between LIC and hepatic T2* in the studied group

3				
Variable	Normal LIC mean ± SD	Abnormal LIC mean ± SD	Mann-Whitney <i>U</i> test	p value
Hepatic T2*	18.4.1 ± 1	4.3 ± 4.2	6.9	0.001**

Table 6 Association between MIC and cardiac T2* in the studied group

Variable	Normal MIC mean ± SD	Abnormal MIC mean ± SD	t test	p value
Cardiac T2*	36.1 ± 7.9	13.9 ± 2.9	3.9	0.001**

Cardiac T2* values showed no relationship with age (p = 0.6). An 8-year-old female was the youngest who developed cardiac siderosis.

The mean hepatic T2* value of the cases was 5.2 ± 4.3 (0.82-18.4) ms with a median of 2.9 ms. The mean LIC was 13.3 ± 9.4 (1.67-37.29) mg/g with a median of 10.7 mg/g. Only 5% of patients (n=2) showed normal iron based on LIC and T2* results. Among 38 patients (95 %) with excess hepatic iron, 11/40 (27.5%) had mild, 32.5% moderate (13/40), and 35% severe (14/40) liver iron overload. A high statistical significance was found regarding the association between LIC and liver T2* (p=0.000) that signify a strong statistical relationship between the LIC and the value of hepatic T2* (Table 4).

Although liver iron loading was moderate to severe in 95% of patients, heart iron content could still be normal in 90% cases (36/40). The mean cardiac T2* was 34.6 \pm 8.8 (range 11.8–52.93, median 34.2) ms and the mean MIC was 0.65 \pm 0.41 (range 0.23–2.21, median 0.53) mg/g. Based on heart T2* and MIC results, only 10% (4/40) of cases showed increased cardiac iron burden. The association of heart T2* with MIC showed a high statistical significance (p = 0.000) (Table 5).

No significant correlation was found between the level of serum ferritin and cardiac iron content based on T2* and MIC (r=-0.1, p=0.4) and (r=0.2, p=0.1), respectively. However, a significant mild positive correlation has been observed between the level of serum ferritin and liver iron loading based on T2* (r=-0.4, p=0.02) and LIC (r=0.56, p=0.01) (Table 6).

A significant but weak correlation (r = 0.3) between liver and heart T2*(p = 0.02) was found; however, no statistically significant correlation was found (r = 0.1) between MIC and LIC (p = 0.5) (Table 7).

Discussion

Beta-thalassemia major is a hereditary genetic disorder of hemoglobin which leads to hemolysis; an effect makes

Table 7 Correlation between hepatic and cardiac investigations of the studied group

Variable	Hepatic T2*		
	r\$	р	SIG
Cardiac T2*	0.5	0.01*	S
		MIC	
	r ^{\$}	p	SIG
LIC	0.1	0.05	NS

^{*}Statistically significant ($p \le 0.05$)

Spearman correlation

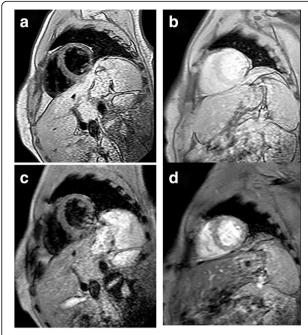


Fig. 2 Gradient echo black blood and white blood T2* static images acquired at TE 1.6 ms (**a**, **b**) and TE 18.8 ms (**c**, **d**) show no decay at T2* signals of the liver or the heart in a thalassemia major patient; normal values of the liver (T2* 18.4 ms, LIC 1.67 mg/g) and heart (T2* 50.4 ms and MIC 0.38 mg/g). The measured serum ferritin was 2000 ng/ml consistent with normal liver and heart findings

these patients need repeated blood transfusions that lead to iron overloading including the liver, heart, spleen, bone marrow, pancreas, and endocrine system [1, 16, 17].

Iron deposition in the heart follows a characteristic pattern; it is greater in the epicardium and more in the

ventricles than the atria [3, 5, 9, 10, 16, 17]. Cardiac dysfunction depends on the quantity of the deposited iron and the extent of fibers involvement. Despite the reversible nature of siderotic cardiomyopathy, the heart is still considered the target lethal organ as 71% of deaths in TM patients are caused by cardiac complications such as iron-induced acute myocarditis and acute heart failure [9–19].

The magnetic resonance signal of the hepatic and cardiac tissues depends on the T1 and T2 relaxation times (TR) of their iron content (Fig. 2). T2* is inversely related to intracellular iron, increased tissue iron displays a moderate decrease in T1 signals and extreme decrease in T2 signal intensities [10, 20, 21].

T2* is a simple, non-invasive and rapid technique that is gained in a single breath-hold [1, 8, 9, 11, 14]. Owing to the late development of the clinical findings and echocardiographic abnormalities, MR-T2* has become the strongest biomarker for simultaneous evaluation of liver and heart iron burden [1, 19] plus prediction of iron-induced cardiac complications such as heart failure and arrhythmia in TM patients [18–20].

Measuring serum ferritin level remains the primary screening test and is still used in monitoring the efficacy of chelation therapy. It has been reported that serum ferritin level greater than 2500 ng/ml is considered an important risk factor for developing ironinduced complications such as liver cirrhosis, heart failure, arrhythmias, impaired growth, and delayed puberty [22–25].

In this study, the level of serum ferritin ranged from 1000 to 7000 ng/ml.

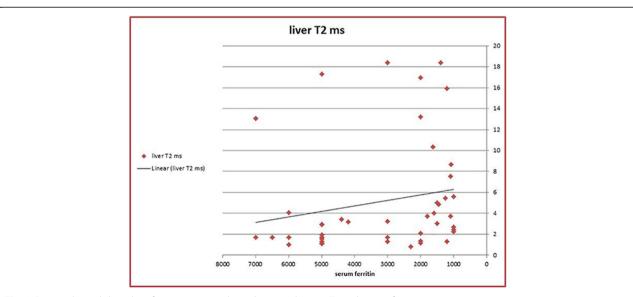
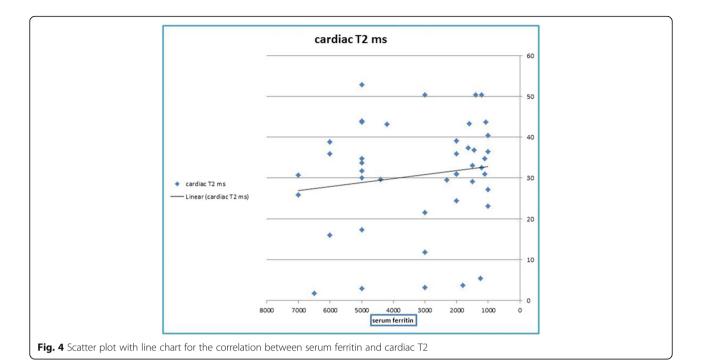


Fig. 3 Scatter plot with line chart for negative correlation between hepatic T2 and serum ferritin



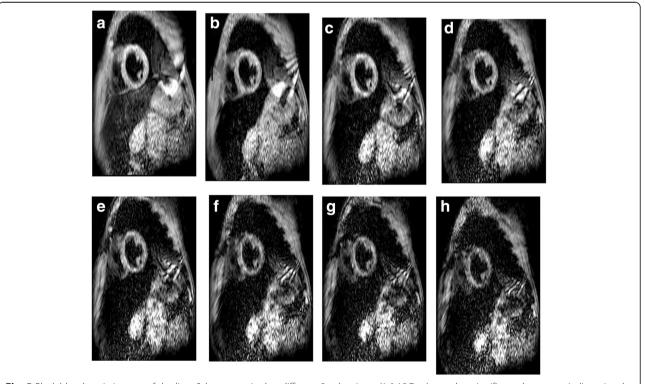


Fig. 5 Black blood static images of the liver & heart acquired at different 8 echo times (1.6-18.7ms) reveals a significant decrement in liver signals with measured values of (T2*: 1.1 ms & LIC: 28.91 mg/g) and normal heart signals with normal (T2*: 43.9 ms & MIC: 0.45 mg/g). The measured serum ferritin was 7000 ng/ml. Findings are consistent with severe hepatic iron deposition with normal cardiac findings

A significant mild positive correlation has been observed between the level of serum ferritin and liver iron loading (Fig. 3); however, no significant correlation was found between the level of serum ferritin and heart iron content based on T2* (Fig. 4), LIC and MIC (Table 4). Also Eghbali et al. [26] studied the association between liver and heart T2* and levels of serum ferritin in TM patients and he reported a correlation between serum ferritin level and liver T2*, but not cardiac T2*. However, Puliyel M et al. 2014 [27] reported that ferritin cannot predict the total body iron changes with a little relevance between cardiac and hepatic iron content and levels of serum ferritin. Anderson et al. 2001 [21] also reported a nonsignificant correlation between cardiac T2* and levels of serum ferritin while Tanner et al. 2005 [7] reported a weak correlation between them.

Wood et al. 2005 [8] and Papakonstantinou et al. 2009 [9] reported that MR-R2* mapping could accurately estimate LIC in transfusion-dependent TM patients. Previous studies found that the frequency of MR-T2* relies on the iron concentration and chelation therapy used [11–13, 18]. In this study, a high statistical significance was found regarding the association between LIC and liver T2* (p = 0.000) (Table 5) and between MIC and cardiac T2* (p = 0.000) (Table 6).

Previous literatures reported that cardiac $T2^*$ of 52 ± 16 ms is the reference range and 20 ms is the minimum value for normal myocardium $T2^*$ [13]. Cardiac siderosis cannot be predicted from the hepatic iron load because liver iron normalizing within 3–6 months which is much faster than the heart [12–14, 18].

We found that although iron-loaded liver was detected in 95% of cases with moderate to severe affection in 67.5% (27/40) of cases, yet the myocardial iron was still normal in (90%) of cases (Fig. 5). However, a significant but weak correlation (r=0.3) has been observed between hepatic and cardiac $T2^*$ (p=0.02). But no significant correlation was found (r=0.1) between MIC and LIC (p=0.5) (Table 7). In agreement with our results, Anderson [12] reported that a marked discordance was observed between hepatic and cardiac iron concentration. Also Di Tucci et al. [28], Tanner et al. [29], Perifanis et al. [30], and Wood et al. [17] reported that no correlation was found among liver $T2^*$, cardiac $T2^*$, and iron concentration levels.

In this study, only 10% of studied cases (4/40) developed iron-loaded heart with either mild (5%; n = 2) or moderate (5%; n = 2) cardiac siderosis which is much less than those reported by Majd et al. [31]

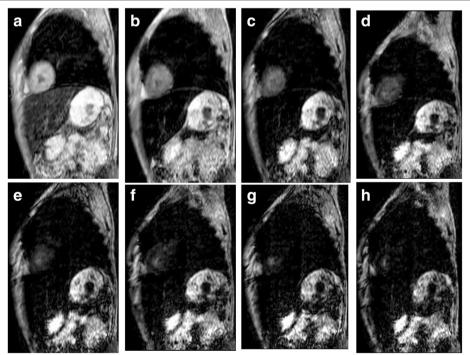


Fig. 6 Coronal images of the liver and heart at 8 different TE (1.6-18.7ms) reveal a significant decay in both hepatic and myocardial signal that increases on longer TE imaging sequences. The measured cardiac values were (T2*: value of 11.8 ms, MIC: 2.21mg/g) and hepatic values were (T2*: 1.3 ms, LIC: 25.33 mg/g). The measured serum ferritin was 3000 ng/ml. These findings are consistent with severe hepatic and moderate cardiac iron deposition. (Note: the moderate cardiac iron overload inspite of the lower level of serum ferritin and liver iron burden in this case compared to the previous case (Fig. 5) reflecting the incompetence among serum ferritin, liver iron burden and cardiac iron load

and Leung et al. [32] who described abnormal cardiac MR-T2* findings in 58% and 50% of patients respectively. This may be attributed to the different chelation regimens used and a better efficacy of ferriprox in removing excess cardiac iron; however, further prospective RCTs on a larger number of patients are needed to confirm this hypothesis.

Josep et al. [33] stated that using echocardiography to measure the diastolic parameters can distinguish early cardiac involvement before the appearance of clinical signs of heart failure. In our study, 10% of cases had excess cardiac iron; however, they presented with normal echocardiographic findings.

Auger and Pennelle [20] reported that assessment of cardiac iron loading should be started between the age of 6 and 10 years and that cardiac siderosis may present at the age of ten by acute heart failure. In this study, the youngest subject who developed cardiac siderosis based on abnormal cardiac $T2^*$ results was an 8-year-old female (Fig. 6). No significant correlation was found between patient age and the development of hepatic or cardiac siderosis (p = 0.6).

This study faced some limitations: first lack of regular follow-up of the patients, second is the inability to perform functional cardiac analysis using MRI owing to unavailable software of the equipment to accomplish that task in our institution, third is the lack of reference standard. Also the large percentage of cases with liver iron overload detected in this study raises the need to re-evaluate the iron chelation strategy used.

Overall, myocardial iron assessment from the assessment of serum ferritin, liver iron, or echocardiography is not reliable enough to adjust the iron chelation strategy in TM patients with risk for cardiac siderosis.

Conclusion

T2* MRI is nowadays the method of choice to early detect, quantify and monitor the hepatic and myocardial iron burden and guiding the chelation therapy to prevent the iron-induced cardiac complications and reduce patients' mortality.

Abbreviations

TM patients: Thalassemia major patients; IRB: Institutional review board; FOV: Field of view; E/A ratio: Early (E) to late (A) ventricular filling velocity; R2*: The gradient echo (the inverse of T2*); TFE: Turbo field echo sequence; RCTs: Randomized clinical trials; LIC: Liver iron concentration; MIC: Myocardial iron concentration

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Authors' contributions

MI carried out the study concept and design, participated in the sequence alignment, and drafted the manuscript. SM carried out the process of

literature search. ZE participated also in the sequence alignment and participated in the design of the study. SM performed the statistical analysis. All authors read and approved the final manuscript.

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Availability of data and materials

This prospective cross-section study included 44 thalassemia pediatric patients from 6 to 15 years old. They were referred from the pediatric department to radio-diagnosis department from February 2015 to January 2019.

Ethics approval and consent to participate

This study was approved by the Institutional Review Board (IRB) of Zagazig University. A written informed consent from all patients' parents before the study were filled and signed, which are also approved by the Institutional Review Board (IRB) of Zagazig University with reference number 3186.

Consent for publication

All patients included in this research gave written informed consent to publish the data contained within this study by their parent.

Competing interests

The authors declare that they have no competing interests.

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