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# Role of diffusion-weighted imaging in carotid plaque vulnerability assessment

Ajay Alex<sup>1</sup>, Anoop Ayyappan<sup>1\*</sup>, Jineesh Valakada<sup>1</sup>, Deepti Narasimhaiah<sup>2</sup>, Shivanesan Pitchai<sup>3</sup> and P. N. Sylaja<sup>4</sup>

# **Abstract**

**Background:** MR plaque imaging is a valuable tool in characterizing carotid atherosclerotic plaque and identifying high-risk features. There are limited data on the role of the widely available single-shot diffusion-weighted imaging (DWI) in plaque characterization along with histological correlation. This study aimed to correlate the plaque characteristics identified by MR imaging in vivo at the level of maximum stenosis with histological plaque characteristics in the postoperative specimen.

**Methods:** Patients who underwent carotid endarterectomy in a tertiary care center during one and half years were prospectively recruited for non-contrast MR carotid plaque imaging (including single-shot EPI-DWI sequence) in a 3 Tesla MRI using a dedicated carotid coil. An experienced radiologist correlated DWI sequence findings with histopathology of postsurgical sections to confirm the high-risk features.

**Results:** Twenty-three patients (mean age 66.1 years  $\pm$  SD 6.25) were evaluated, of which 65% were males and 96% were symptomatic. Apparent diffusion coefficient (ADC) values in location of plaques could differentiate histopathological unstable from stable plaques (0.83  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s vs 1.7  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s; p 0.001), with a sensitivity and specificity of 75% and 79%, respectively, at an ADC cutoff of 1.24  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s. Plaques with and without lipid-rich necrotic core (0.86  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s vs 1.44  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s; p 0.042) as well as intraplaque hemorrhage could be differentiated (0.751  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s vs 1.352  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s; p 0.037) using the apparent diffusion coefficients.

**Conclusion:** The widely available single-shot EPI-DWI in assessing plaque characteristics in carotid stenosis is promising and correlated with histopathological features. Diffusion-weighted imaging will be a helpful adjunct in patients when contrast administration is intolerable.

**Keywords:** Carotid artery stenosis, Carotid atherosclerotic plaque, Diffusion-weighted imaging, Carotid endarterectomy

# **Background**

MR imaging of the carotid plaque has evolved as an essential tool for detecting high-risk plaque characteristics, mainly since 25–50% of ischemic strokes are caused by an unstable carotid artery plaque [1]. There is a growing awareness that stenosis severity alone has limited value in predicting plaque stability. Various molecular

processes have shown to be associated with plaque vulnerability, independent of the degree of stenosis. Symptomatic patients were more likely to have a thin fibrous cap (30–50%), intra-plaque hemorrhage (45–60%), a large lipid core (50–80%), and a complex morphology (61.5%) in MR imaging [2, 3]. Additionally, these characteristics are independent predictors of future ischemic events. Though contrast-enhanced MRI sequence is needed for characterizing plaque, recently published American Society of Neuroradiology consensus statement recommends non-contrast protocols as well [4]. Standard single-shot EPI-DWI with ADC measurement has been evaluated only sparingly for plaque assessment in the published

Full list of author information is available at the end of the article



<sup>\*</sup>Correspondence: anoop123a@gmail.com

<sup>&</sup>lt;sup>1</sup> Department of Imaging Sciences and Interventional Radiology, Sree Chitra Tirunal Institute for Medical Sciences and Technology, Trivandrum, Kerala 695011. India

literature with most studies having in vitro evaluation and small samples. This study aims to evaluate the utility of comparing single-shot EPI-DWI at the level of maximum stenosis for plaque vulnerability assessment compared to the histopathological specimen and identify the high-risk features that are likely to translate into variations in ADC values. Single-shot EPI-DWI was chosen as part of the study since it is the most widely available diffusion sequence across vendors, thus enabling its universal application compared to the newer DWI sequences. Since DWI does not require contrast administration, it can be an adjunct tool in patients who require avoidance of contrast agents as in chronic kidney disease, allergies, and serial follow-up on medical management.

#### Methods

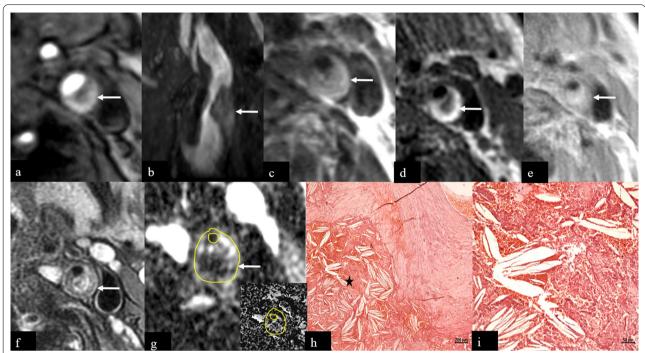
This was a prospective study conducted from October 2018 to June 2020 in a single center after obtaining the institutional ethics committee approval. Informed written consent was obtained from all the participants. Twenty-seven consecutive patients who sought medical care after at least one major or minor cerebrovascular event and having a moderate to severe carotid artery stenosis (>50% stenosis) were planned for carotid endarterectomy after a multidisciplinary stroke team meeting according to the European Society for Vascular Surgery guidelines of 2017 [5]. Patients not consenting for the MR examination and patients with a pacemaker or metallic implant in the body were excluded from the study. The study patients underwent carotid plaque MR imaging in a 3.0 Tesla machine (General Electric Discovery 750E, GE Healthcare, Waukesha, WI, USA) using a 6-channel carotid coil. Before placing the patient in the MR scanner, the level of the maximum carotid stenosis was marked over the skin using ultrasonography to ensure optimal carotid surface coil position and resultant better signal. The sequences used included T1, T2, T2FS, TOF, PD, and DWI (total acquisition time ~ 23.5 min). The protocols for the primary sequences were as described in previous papers [6–8]. The standard diffusion-weighted echo-planar sequence was used as part of the study to provide a degree of robustness against the involuntary patient motion and keep acquisition times clinically acceptable. In DWI acquisition, saturation bands were positioned superiorly and inferiorly to suppress signals from in-flowing blood and anteriorly and posteriorly to minimize wraparound artifact. The b values used in the study were 10, 500, and 1000. A baseline b value of 10 was taken instead of 0 for nulling the blood flow signals resulting from neovascularization of the plaque which might confound the effect of necrosis or hemorrhage [9]. Other DWI parameters were TE 71.5 ms; TR 3800 ms; matrix size  $120 \times 60$ ; section thickness 2 mm; and acquisition time 4.2 min. Zero interpolation algorithm (ZIP) was applied in T2, T2 FS, and PD sequences. Images were assessed on the GE Advantage workstation (GE Healthcare, Waukesha, WI, USA) version 4.6 using the GenIQ application. The site of maximum carotid plague thickness was identified on 3D TOF MRA in the workstation. A corresponding cross section of the carotid artery image in the DWI sequence was used to measure the ADC values of the plaque. For ADC map generation, ROI was drawn after correlation with T2 and T2 FS sequences in corresponding slices to confirm the plaque's outer and inner limits (Figs. 1, 2, 3). These images were analyzed by a reader with more than 5 years of experience in interpreting diagnostic vascular imaging studies. The DWI and ADC images were analyzed for the image-quality-cum diagnostic confidence and graded using a 4-point scale. An image-quality rating from 1 to 4, with 1 being poor and 4 being excellent, was assigned before the review. Studies with an overall image quality rating of 1 and 2 were excluded. Further, the patient underwent surgery on an average of 4 days after magnetic resonance imaging.

A total of 27 study patients were recruited of which 92.6% of the cases had adequate image quality to interpret plaque characteristics. Two participants were excluded due to the suboptimal image quality in MRI, and two more were excluded due to inadequacy of specimen for histopathological assessment.

# **Histology protocol**

The endarterectomy specimens were fixed in buffered formalin immediately after surgery. Serial cross sections were taken from the specimens at 2-mm intervals and processed as per standard protocols in the histopathology laboratory. For all cases, the entire endarterectomy specimen was processed. However, the maximum carotid luminal narrowing level was used to align with corresponding MR sections for correlation. Hematoxylin and eosin (H&E), Masson's trichrome (MAT), and elastic van Gieson (EVG) stains were performed on 5-µm sections. The pathologist assessed all the slides, and the histological features were scored using a semiquantitative method as described by Lovett et al. [10, 11]. For analysis, probably and definitely unstable plaques with grade 3/4 lipid necrotic core and intraplaque hemorrhage were categorized as being vulnerable and the rest were categorized as being stable. For analysis, only large lipid necrotic core and intraplaque hemorrhage were considered instability features. A similar criterion was also followed in imaging studies.

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**Fig. 1** Carotid MR images of an ICA plaque in a 70-year-old diabetic male who had symptomatic left MCA stroke, who had NIHS score of 8 at admission, and no prior cerebrovascular events were detected to have 72% stenosis in MR TOF (**a**, **b**), with the ICA plaque (arrows) showing TOF(A) and T1 (**c**) hyperintensity indicative of intraplaque hemorrhage. The plaque appeared predominantly hyperintense in T2 (**d**), PD (**e**), and T2FS (**f**). DWI image (**g**) showing plaque with inset showing ADC map with margins of vessel wall and vessel lumen demarcated by line tracing adapted from corresponding T2FS image. The plaque had average ADC value of  $0.83 \times 10^{-3}$  mm<sup>2</sup>/s. Histopathological images (**h**, **i**) of the same plaque showing intraplaque hemorrhage (\*) containing RBCs admixed with few cholesterol clefts. (Hematoxylin and eosin, **h** original magnification  $50 \times$ , scale bar  $200 \mu m$ , **i** original magnification  $200 \times$ , scale bar  $50 \mu m$ )

# Statistical analysis

Each patient contributed only 1 set of observations (i.e., from only one carotid artery) to the dataset for analysis. Statistical analysis was performed using SPSS Version 23.0 (IBM, Armonk, NY) software. Descriptive statistical tools were used for basic frequencies of plaque characteristics and patient demographics. An independent sample t test was used for the comparison of mean ADC values between each of the plaque characteristics and overall plaque vulnerability. Receiver operating characteristic (ROC) analysis was performed to assess optimal ADC value in detecting plaque vulnerability.

#### **Results**

# $Demographics \ and \ risk \ factors \ in \ the \ study \ population$

The demographic and clinical data of the final 23 patients of the study are summarized in Table 1. 17.3% of the study patients had moderate (50–70%) carotid stenosis. 69.5% of the plaques revealed unstable features on histopathological evaluation.

# DWI and ADC value relation with plaque composition

The mean ADC values could differentiate vulnerable from non-vulnerable plaques (0.83  $\times\,10^{-3}$  mm²/s vs.  $1.7\times10^{-3}$  mm²/s; p 0.001).

Besides, it also revealed a significant difference in mean ADC values in plaques with lipid necrotic core  $(0.86\times10^{-3}~mm^2/s)$  and absent lipid necrotic core  $(1.44\times10^{-3}~mm^2/s).$ 

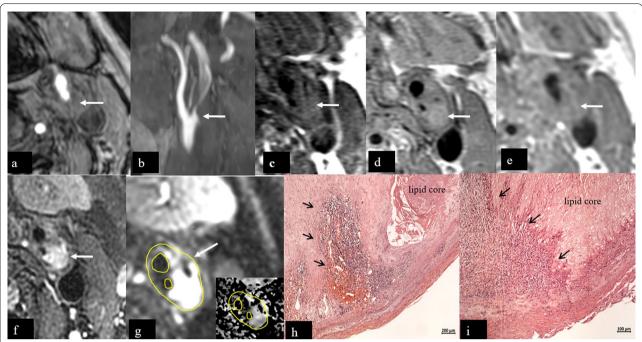
The mean ADC values between plaques with hemorrhage  $(0.751\times10^{-3}~\text{mm}^2/\text{s})$  and without hemorrhage  $(0.751\times10^{-3}~\text{mm}^2/\text{s})$  was also statistically significant (p=0.037). The findings are summarized in Table 2.

ROC analysis (Fig. 4) with an ADC value of  $1.1145 \times 10^{-3}$  mm<sup>2</sup>/s had a sensitivity of 71.4% and specificity of 81.2%. Representative cases of vulnerable and non-vulnerable plaques are shown in Figs. 1, 2 and 3, respectively.

# Discussion

Identifying the plaques as vulnerable will allow a more vigilant follow-up strategy and early interventions to these plaques despite presenting as mild stenosis or as incidental findings. ADC was found to be better than

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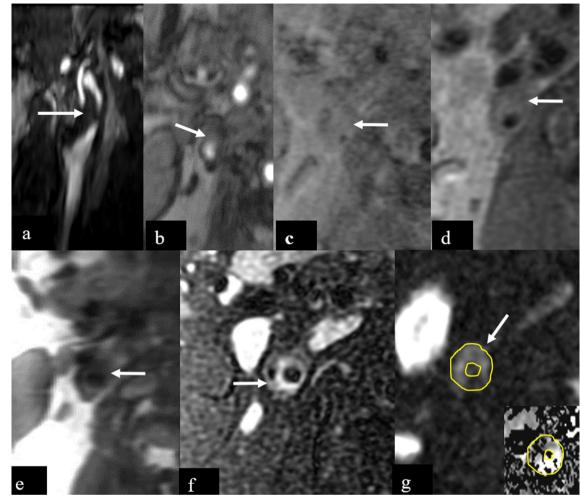
**Fig. 2** Carotid MR images of a 66-year hypertensive female with left ICA stenosis detected following right upper limb paresis. TOF images (**a**, **b**) showed mildly hyperintense plaque (arrows) involving carotid bulbs extending into the proximal left ICA causing  $\sim$  80% stenosis. T1 image (**c**) showed the plaque to have iso-hyperintense areas, which showed hyperintensity in PD (**d**) compared to T2 (**e**), suggesting lipid-rich plaque. The plaque, as identified better in a T2 FS (**f**) image, showed hyperintense areas in and DWI (**g**) with an ADC value (inset, **g**) of 0.41 x 10<sup>-3</sup>mm<sup>2</sup>/sec. Post endarterectomy, histopathological analysis (**h**, **i**) showed necrotic lipid core with inflammatory cell infiltrate (arrows in **h** - Haematoxylin and Eosin, original magnification 50X, Scale bar 200  $\mu$ m, **i** - Original magnification 100X, Scale bar 100  $\mu$ m).

even T1/T2 mapping techniques in differentiating fibrous plaques and lipid-rich necrotic plaques by Clarke et al. [12]. Our study used the plague characteristics at the maximum stenosis in MRI and histopathology for comparison; on the contrary, most of the previous studies that assessed DWI have used average ADC value from multiple levels of plaque for evaluation of plaque composition [9, 13, 14]. This was based on the notion that the most aggressive part of the plaque would be at level of maximum stenosis and the ADC characteristics of that level will predict the vulnerability in the most representative manner. Our study showed that the EPI-DWI sequence with ADC measurement is effective in differentiating histologically stable and unstable plaques. A significant difference in mean ADC values between vulnerable and non-vulnerable plaques was depicted with a cutoff of  $1.24 \times 10^{-3}$  mm<sup>2</sup>/s, with a sensitivity of 75% and specificity of 79%. This was despite the overall moderate image quality compared to a few of the recent studies which used 3D DWI, at the cost of increased acquisition time. DWI was found to be applicable for the assessment of carotid plaque by Kim et al. [15] using 2D ss-IMIV-DWEPI sequence with both in vivo and ex vivo mean ADC measurement on 8 study patients and documented detection of the lipid necrotic core. In their study, the mean ADC for normal vessel wall and hemorrhage was  $1.27 \times 10^{-3}$  and  $0.98 \times 10^{-3}$  mm<sup>2</sup>/s, respectively. 2D ss-IMIV-DWEPI was used to avoid the geometrical distortion in EPI. 3D DWI was used for a better depiction of the vessel wall by Xie et al. [13], but no histological correlation was done as part of the study.

In our study, plaques with and without lipid-rich necrotic core could also be differentiated. Earlier ex vivo studies had already evaluated the utility of decreased ADC in necrotic core detection, with only very limited in vivo studies with a relatively small sample size [9, 16]. In the study by Kim et al., the lipid-rich necrotic core had a mean ADC of  $0.38 \times 10^{-3}$  mm²/s as against our values of  $0.86 \times 10^{-3}$  mm²/s, which was similar to values in the study by Ota et al. [9] Our ADC values also were similar to the results by Young et al., with the ADC value for lipid core being  $0.73 \times 10^{-3}$  mm²/s using EPI-DWI sequence [14].

The initial study done by Yao et al. on intraplaque hemorrhage detection using ADC values in 3T MRI showed that the mean ADC value in IPH was  $0.985\pm0.376~\mu m^2$  [17]. However, the study did not have histopathological evaluation. In the study by Kim et al. and Ota et al., there

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**Fig. 3** Carotid MR images of a 65-year-old male with left hemiparesis, who was detected to have right ICA 80% stenosis (arrows). His NIHS at admission was 6, with a total of 2 cerebrovascular events before surgery. TOF images (**a**, **b**) showing right ICA stenosis with axial TOF showing a largely preserved periluminal dark band indicative of intact fibrous cap. T1 image (**c**) showed mildly increased signal with T2 (**d**) and PD (**e**), showing the plaque to have largely similar intensities. T2 FS (**f**) also showed the luminal stenosis with DWI image (**g**) with an ADC value of 1.290  $\times$  10<sup>-3</sup> mm<sup>2</sup>/s (inset in q)

was an overlap between ADC values of hemorrhage and lipid-rich necrotic core [9, 15]. Moreover, in the study by Ota et al., there was a considerable difference in ADC values between the two institutions where the study was done. We found a considerable overlap of ADC values within hemorrhage and lipid-rich necrotic cores possibly due to the various stages of the hemorrhage, coexistent lipid necrosis with hemorrhage, and inherent errors of the sequence used for assessment.

Compared to the previous studies which did histopathological correlations, our study had a reasonable sample size [7, 12]. The technical ease of doing endarterectomy was similar in both subsets of plaques. The vulnerable plaque carries a slightly higher theoretical risk for distal emboli

while dissecting the vessel; however, no such differences were noticed in our patients. The use of readily available EPI-DWI makes the sequence suitable for routine use, unlike the majority of the studies which have used various modifications of the sequence.

# Limitations

The limited number of patients in our study would have reduced our sensitivity in differentiation of various pathologies. All our study patients had moderate to severe stenosis ( $\geq 50\%$ ); thus, visualization of the plaque in our protocols was not much of an issue. Hence, its applicability in patients with 50-70% stenosis may be potentially used for decision-making

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**Table 1** Demographic and clinical data of the study (n = 23)

Gender	Male—15; Female—8		
Age	Median age 66 years (range 50–74 years) Symptomatic—22; asymptomatic—1		
Clinical status			
Risk factors			
	Present	Absent	
Smoking	8	15	
Diabetes mellitus	15	8	
Alcoholism	6	17	
Hypertension	20	3	
CAD	0	23	
Dyslipidemia	11	12	
CKD	0	23	
POVD	2	21	
MRI evaluation and histopathology			
Mean number of days between the last cerebrovascular event and carotid plaque $\ensuremath{MRI}$	57 days		
The mean number of days between MRI and carotid endarterectomy	4 days		
Degree of carotid stenosis			
50–70% stenosis	4		
More than 70% stenosis	19		
Plaque vulnerability in histopathological evaluation			
Vulnerable plaque	16		
Stable plaque	7		

CAD coronary artery disease, CKD chronic kidney disease, POVD peripheral occlusive vascular disease

Table 2 Mean ADC values assessed in each of the carotid plaques in the particular histological characteristics

	No. of study patients	Mean ADC value	Standard error	95% CI	<i>p</i> value
Overall plaque vulnera	bility				
Vulnerable	16	$0.83 \times 10^{-3}$	$0.10 \times 10^{-3}$	$0.405 \times 10^{-3} - 1.44 \times 10^{-3}$	0.001
Non-vulnerable	7	$1.7 \times 10^{-3}$	$0.29 \times 10^{-3}$		
Lipid-rich necrotic core	(LRNC)				
LRNC present	13	$0.86 \times 10^{-3}$	$0.13 \times 10^{-3}$	$0.022 \times 10^{-3} - 1.14 \times 10^{-3}$	0 .042
LRNC absent	10	$1.44 \times 10^{-3}$	$0.26 \times 10^{-3}$		
Intra-plaque hemorrho	age (IPH)				
IPH present	9	$0.751 \times 10^{-3}$	$0.111 \times 10^{-3}$	$0.038 \times 10^{-3} - 1.164 \times 10^{-3}$	0.037
IPH absent	14	$1.352 \times 10^{-3}$	$0.203 \times 10^{-3}$		

ADC apparent diffusion coefficient

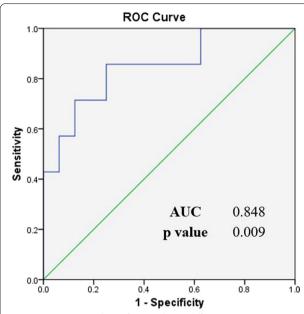
for revascularization. However, the utility in patients with < 50% stenosis with reduced plaque burden may be limited. Inter- and intraobserver variability was not assessed in this study, which would have evaluated the reproducibility of this modality. The unavailability of the newer motion correction sequences may also have influenced image acquisition. The inclusion of only > 50% stenosis patients who mostly had prior cerebrovascular events is in itself a selection bias, as is the case in all similar studies in the literature. Evaluation with much

larger samples may be vital in validating the findings and their utility.

#### **Conclusions**

The standard DWI with ADC assessment at the level of maximum stenosis of the carotid artery in delineating plaque characteristics correlates with histopathology. Diffusion-weighted imaging will be a helpful adjunct in patients when contrast administration is intolerable.

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**Fig. 4** ROC curve analysis of ADC value in differentiating non-vulnerable plaque from vulnerable plaque

#### **Abbreviations**

3T: 3-Tesla; ADC: Apparent diffusion coefficient; DWI: Diffusion-weighted imaging; EPI: Echo planar imaging; H & E: Hematoxylin and eosin; IPH: Intra-parenchymal hemorrhage; MRI: Magnetic resonance imaging; PD: Proton density; ss-IMIV-DWEPI: Single-shot interleaved multislice inner volume diffusion-weighted echo planar imaging; ROC: Receiver operating characteristic; ROI: Region of interest; TOF: Time of flight; TR: Repetition time.

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Not applicable.

#### **Author contributions**

AA contributed to methodology, investigation, writing—original draft preparation, and data curation. AAY helped in conceptualization, methodology, writing—original draft preparation, reviewing and editing, validation, and funding acquisition. PNS was involved in conceptualization, writing—reviewing and editing, and validation. DN and SP performed investigation, visualization, and validation. JV performed reviewing and editing. All authors read and approved the final manuscript.

#### Funding

The study received fund from the Institute Technical Development Fund for MRI examinations.

#### Availability of data and materials

The data are available from institutes Picture Archiving and Communication System after taking Institutional Ethical Approval.

# **Declarations**

# Ethics approval and consent to participate

Institutional Ethical Approval was obtained. Consent to participate was obtained as written informed consent from all participants.

#### Consent for publication

Appropriate consents for publishing the clinical and imaging details of the patient were obtained.

#### **Competing interests**

The authors declare that they have no competing interests.

#### **Author details**

<sup>1</sup>Department of Imaging Sciences and Interventional Radiology, Sree Chitra Tirunal Institute for Medical Sciences and Technology, Trivandrum, Kerala 695011, India. <sup>2</sup>Department of Pathology, Sree Chitra Tirunal Institute for Medical Sciences and Technology, Trivandrum, Kerala, India. <sup>3</sup>Department of Vascular Surgery, Sree Chitra Tirunal Institute for Medical Sciences and Technology, Trivandrum, Kerala, India. <sup>4</sup>Department of Neurology, Sree Chitra Tirunal Institute for Medical Sciences and Technology, Trivandrum, Kerala, India.

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